

# Basics of X-ray scattering by solutions

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## Biological SAXS @ EMBL-HH

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### Major tasks:

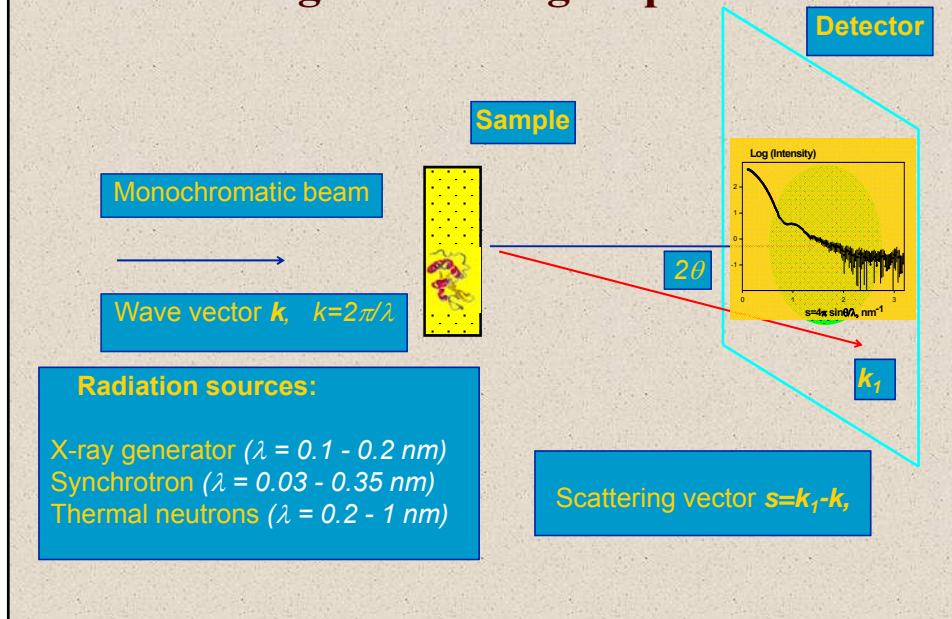
- ❑ Development of data analysis methods
- ❑ Running and developing SAXS beamlines
- ❑ User support and collaborative projects
- ❑ Education and training

## Modern synchrotron SAXS



## General principles of solution SAXS

### Small-angle scattering: experiment



## Scattering by matter

- **X-rays** are scattered mostly by electrons
- **Thermal neutrons** are scattered mostly by nuclei
- Scattering amplitude from an ensemble of atoms  $A(\mathbf{s})$  is the Fourier transform of the scattering length density distribution in the sample  $\rho(\mathbf{r})$
- Experimentally, scattering intensity  $I(\mathbf{s}) = [A(\mathbf{s})]^2$  is measured.

## Notations

The momentum transfer (i.e. the modulus of the scattering vector) is denoted here as  $s=4\pi \sin(\theta)/\lambda$

There are also different letters used, like

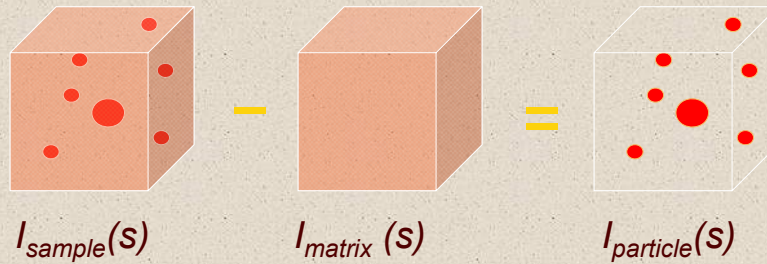
$$Q = q = s = h = k = 4\pi \sin(\theta)/\lambda$$



Sometimes, the variable  $S=2\sin\theta/\lambda = 2\pi s$  is used, and to add to the confusion, also denoted as “s”, or  $\mu$  or yet another letter. Always check the definition for the momentum transfer in a paper

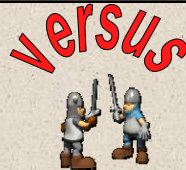


## Small-angle scattering: contrast



- ♦ To obtain scattering from the particles, matrix scattering must be subtracted, which also permits to significantly reduce contribution from parasitic background (slits, sample holder etc)
- ♦ **Contrast**  $\Delta\rho = \langle\rho(r) - \rho_s\rangle$ , where  $\rho_s$  is the scattering density of the matrix, may be very small for biological samples

**X-rays**



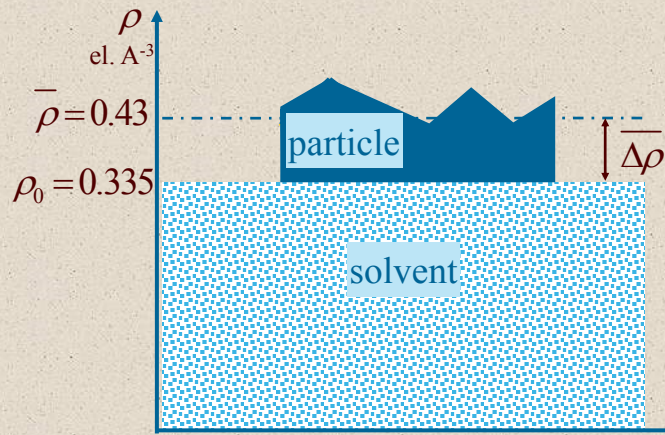
**neutrons**

- **X-rays:** scattering factor increases with atomic number, no difference between H and D
- **Neutrons:** scattering factor is irregular, may be negative, huge difference between H and D

Element	H	D	C	N	O	P	S	Au
At. Weight	1	2	12	14	16	30	32	197
N electrons	1	1	6	7	8	15	16	79
$b_x, 10^{-12} \text{ cm}$	0.282	0.282	1.69	1.97	2.16	3.23	4.51	22.3
$b_N, 10^{-12} \text{ cm}$	-0.374	0.667	0.665	0.940	0.580	0.510	0.280	0.760

**Neutron contrast variation**

## Contrast of electron density



In the equations below we shall always assume that the solvent scattering has already been subtracted

## Solution of particles

The diagram illustrates the relationship between a solution, a motif, and a lattice. A box containing many dots (representing a solution) is equal to a box containing one dot (representing a motif) multiplied by a box containing many dots (representing a lattice). Below this, the same relationship is written in mathematical terms.

<b>Solution</b>	<b>=</b>	<b>Motif (protein)</b>	<b>*</b>	<b>Lattice</b>
$\Delta\rho(\mathbf{r})$		$\Delta\rho_p(\mathbf{r})$	<b>*</b>	$d(\mathbf{r})$
$F(\mathbf{c}, s)$		$F(0, s)$	<b>.</b>	$\delta(\mathbf{c}, s)$

## Solution of particles

For spherically symmetrical particles

$$I(c,s) = I(0,s) \times S(c,s)$$

form factor      structure factor  
of the **particle**      of the **solution**

Still valid for globular particles though over a restricted s-range

## Solution of particles

- 1 – *monodispersity*: identical particles
- 2 – size and shape polydispersity
- 3 – *ideality* : no intermolecular interactions
- 4 – non ideality : existence of interactions between particles

*In the following, we make the double assumption 1 and 3*

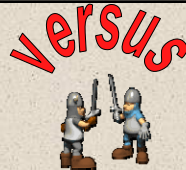
## Ideal and monodisperse solution

$$A(\mathbf{s}) = \mathfrak{T}[\Delta\rho(\mathbf{r})] = \int_V \Delta\rho(\mathbf{r}) \exp(i\mathbf{s}\mathbf{r}) d\mathbf{r}$$

Particles in **solution**  $\Rightarrow$  thermal motion  $\Rightarrow$  particles have random orientations to X-ray beam. The sample is *isotropic*. Therefore, only the *spherical average* of the scattered intensity is experimentally accessible.

Ideality and monodispersity  $I(s) = N i_1(s)$

Crystal



solution

$$I(\mathbf{c}, \mathbf{s}) = I(0, \mathbf{s}) \times S(\mathbf{c}, \mathbf{s})$$

For an ideal crystal,  
 $I(\mathbf{s})$  is the three-dimensional  
 scattering intensity from  
 the unit cell

$S(\mathbf{s})$  is a sum of  $\delta$ -functions  
 along the directions of the  
 reciprocal space lattice

$$\mathbf{s} = (h\mathbf{a}^* + k\mathbf{b}^* + l\mathbf{c}^*)$$

For an ideal dilute solution,  
 $I(\mathbf{s}) = I(s)$  is the orientationally  
 averaged intensity of the  
 single particle

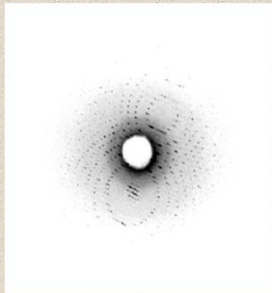
$S(s)$  is equal to unity



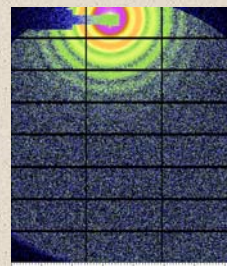
# Crystal *versus* solution



For an ideal crystal, measured signal is amplified into specific directions allowing measurements to high resolution ( $d \approx \lambda$ )



For an ideal dilute solution,  $I(\mathbf{s})$  is isotropic and concentrates around the primary beam (this is where the name “small-angle scattering” comes from): low resolution ( $d \gg \lambda$ ).



## Main equations and overall parameters



## Relation between real and reciprocal space

Using the overall expression for the Fourier transformation one obtains for the spherically averaged single particle intensity

$$I(s) = \left\langle A(\mathbf{s}) A^*(\mathbf{s}) \right\rangle_{\Omega} = \left\langle \int_V \int_V \Delta\rho(\mathbf{r}) \Delta\rho(\mathbf{r}') \exp\{i\mathbf{s}(\mathbf{r} - \mathbf{r}')\} d\mathbf{r} d\mathbf{r}' \right\rangle_{\Omega}$$

or, taking into account that  $\langle \exp(i\mathbf{s}\mathbf{r}) \rangle_{\Omega} = \sin(sr)/sr$  and integrating in spherical coordinates,

$$I(s) = 4\pi \int_0^{D_{\max}} r^2 \gamma(r) \frac{\sin sr}{sr} dr$$

where

$$\gamma(r) = \left\langle \int \Delta\rho(\mathbf{u}) \Delta\rho(\mathbf{u} + \mathbf{r}) d\mathbf{u} \right\rangle_{\omega}$$

## Distance distribution function

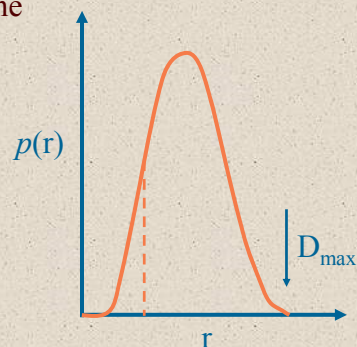
$$p(r) = r^2 \gamma(r) = r^2 \gamma_0(r) V \rho^2$$

$\gamma_0(r)$  : **probability** of finding a point at  $r$  from a given point

number of el. vol.  $i \propto V$  - number of el. vol.  $j \propto 4\pi r^2$

**number** of pairs  $(i,j)$  separated by the

distance  $r \propto 4\pi r^2 V \gamma_0(r) = (4\pi/\rho^2) p(r)$



## Debye formula

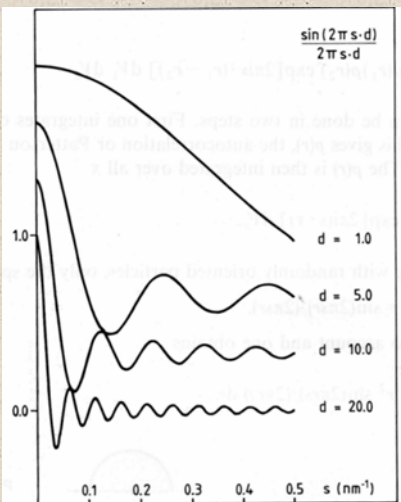
If the particle is described as a discrete sum of elementary scatterers, (e.g. atoms) with the atomic scattering factors  $f_i(s)$  the spherically averaged intensity is

$$I(s) = \sum_{i=1}^K \sum_{j=1}^K f_i(s) f_j(s) \frac{\sin(sr_{ij})}{sr_{ij}}$$

where  $r_{ij} = |\mathbf{r}_i - \mathbf{r}_j|$

The Debye (1915) formula is widely employed for model calculations

## Contribution of distances to the scattering pattern



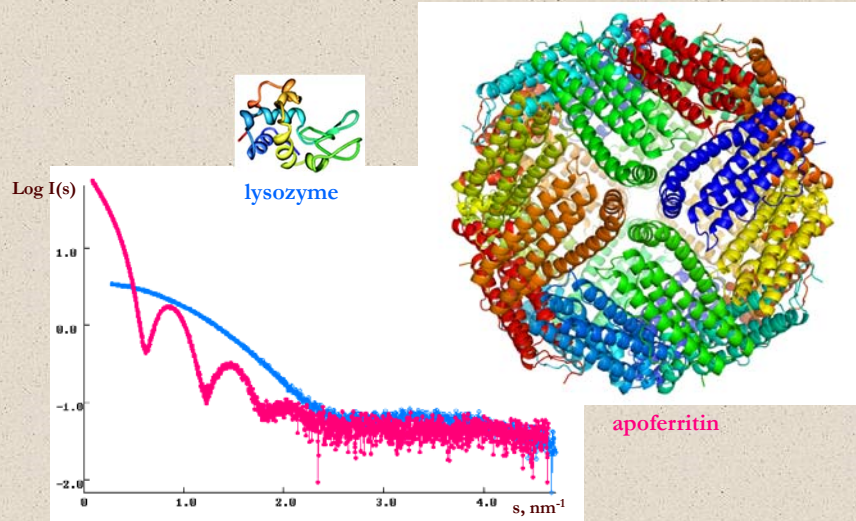
In isotropic systems, each distance  $d = r_{ij}$  contributes a  $\sin x/x$ -like term to the intensity.

**Large distances** correspond to high frequencies and only contribute at **low angles** (i.e. at low resolution, where particle shape is seen)

**Short distances** correspond to low frequencies and contribute over a large angular range.

Clearly at **high angles** their contribution dominates the scattering pattern.

## Small and large proteins: comparison



### Guinier law

Near  $s=0$  one can insert the McLaurin expansion  $\sin(sr)/sr \approx 1 - (sr)^2/3! + \dots$  into the equation for  $I(s)$  yielding

$$I(s) = I(0) \left[ 1 - \frac{1}{3} R_g^2 s^2 + O(s^4) \right] \cong I(0) \exp\left(-\frac{1}{3} R_g^2 s^2\right)$$

This is a classical formula derived by Andre Guinier (1938) in his first SAXS application (to defects in metals). The formula has two parameters, forward scattering and the radius of gyration

$$I(0) = \int_V \int_V \Delta\rho(\mathbf{r}) \Delta\rho(\mathbf{r}') d\mathbf{r} d\mathbf{r}' = 4\pi \int_0^{D_{\max}} p(r) dr = (\Delta\rho)^2 V^2$$

$$R_g = \left[ \frac{\int_0^{D_{\max}} r^2 p(r) dr}{2 \int_0^{D_{\max}} p(r) dr} \right]^{-1}$$

ideal  
monodisperse

### Intensity at the origin

$$i_1(0) = \int_{V_r} \int_{V_{r'}} \Delta\rho(\mathbf{r}) \Delta\rho(\mathbf{r}') dV_r dV_{r'}$$

$$i_1(0) = \Delta m^2 = (m - m_0)^2 = \left[ \frac{M}{N_A} \bar{v}_P (\rho - \rho_0) \right]^2$$

$c = \frac{NM}{N_A V}$  is the concentration (w/v), e.g. in mg.ml<sup>-1</sup>

$$I(0) = \frac{cMV}{N_A} \left[ \bar{v}_P (\rho - \rho_0) \right]^2$$

ideal  
monodisperse

### Intensity at the origin

If : the concentration  $c$  (w/v),  $\bar{v}_P$ ,  
the partial specific volume  $\bar{v}_P$ ,  
the intensity on an absolute scale,  
i.e. the number of incident photons  
are known,

Then, the **molecular weight** of the particle can be  
determined from the value of the intensity at the origin

In practice, MM can be determined from the data on  
relative scale by comparison with  $I(0)$  of a reference protein  
(e.g. BSA, lysozyme or cytochrom C)

ideal  
monodisperse



## Radius of gyration

**Radius of gyration :** 
$$R_g^2 = \frac{\int_V \Delta\rho(\mathbf{r}) r^2 dV_r}{\int_V \Delta\rho(\mathbf{r}) dV_r}$$

$R_g$  is the quadratic mean of distances to the center of mass weighted by the contrast of electron density.

$R_g$  is an *index of non sphericity*.

For a given volume the smallest  $R_g$  is that of a sphere :

$$R_g = \sqrt{\frac{3}{5}} R$$

Ellipsoid of revolution (a, b)

$$R_g = \sqrt{\frac{2a^2 + b^2}{5}}$$

Cylinder (D, H)

$$R_g = \sqrt{\frac{D^2}{8} + \frac{H^2}{12}}$$

ideal  
monodisperse

## Virial coefficient

In the case of moderate interactions, the intensity at the origin varies with concentration according to :

$$I(0, c) = \frac{I(0)_{ideal}}{1 + 2A_2Mc + \dots}$$

Where  $A_2$  is the second virial coefficient which represents pair interactions and  $I(0)_{ideal}$  is  $\propto$  to  $c$ .

$A_2$  is evaluated by performing experiments at various concentrations  $c$ .

$A_2$  is  $\propto$  to the slope of  $c/I(0, c)$  vs  $c$ .

To obtain  $I(0, s)$ , this extrapolation to infinite dilution is performed for different angles

## Guinier plot example

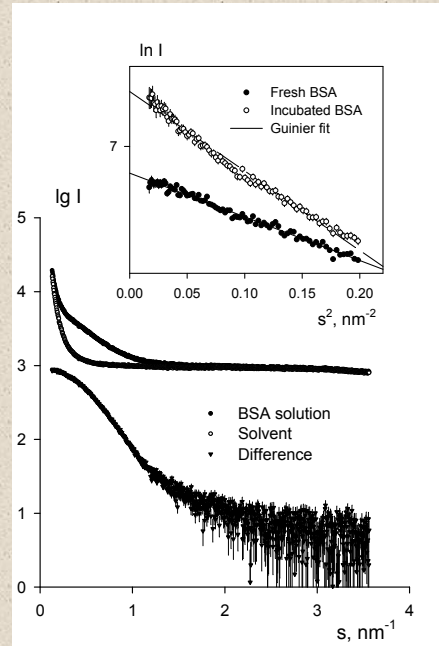
The law is generally used under its log form :

$$\ln[I(s)] = \ln[I(0)] - [sR_g]^2 / 3$$

A linear regression yields two parameters :  $I(0)$  (y-intercept)  
 $R_g$  from the slope

**Validity range :**  
 $0 < sR_g < 1.3$

ideal  
monodisperse



## Rods and platelets

In the case of very elongated particles, the radius of gyration of the cross-section can be derived using a similar representation, plotting this time  $sI(s)$  vs  $s^2$

$$sI(s) \cong I_c(0) \exp\left(-\frac{1}{2} R_c^2 s^2\right)$$

In the case of a platelet, a thickness parameter is derived from a plot of  $s^2 I(s)$  vs  $s^2$  :

$$s^2 I(s) \cong I_T(0) \exp\left(-R_t^2 s^2\right)$$

with  $R_t = T/\sqrt{12}$      $T$  : thickness

ideal  
monodisperse

## Distance distribution function

$$p(r) = \frac{r^2}{2\pi^2} \int_0^\infty s^2 I(s) \frac{\sin sr}{sr} dr$$

In theory, calculation of  $p(r)$  from  $I(s)$  is simple.

**Problem** :  $I(s)$  - is only known over  $[s_{\min}, s_{\max}]$  : truncation  
 - is affected by experimental errors and possible instrumental distortions due to the beam-size and the bandwidth  $\Delta\lambda/\lambda$  (neutrons)

$\Rightarrow$  Fourier transform of *incomplete and noisy data* is an *ill-posed problem*.

**Solution** : Indirect Fourier Transform (suggested by O. Glatter, 1977).

$p(r)$  is parameterized on  $[0, D_{\max}]$  by a linear combination of orthogonal functions, where  $D_{\max}$  is the particle diameter.

Implemented in several programs, including GNOM (part of ATSAS)

ideal  
monodisperse

## Distance distribution function

The radius of gyration and the intensity at the origin are derived from  $p(r)$  using the following expressions :

$$R_g^2 = \frac{\int_0^{D_{\max}} r^2 p(r) dr}{2 \int_0^{D_{\max}} p(r) dr} \quad \text{and} \quad I(0) = 4\pi \int_0^{D_{\max}} p(r) dr$$

This alternative estimate of  $R_g$  makes use of the whole scattering curve, and is much less sensitive to interactions or to the presence of a small fraction of oligomers.

Comparison of both estimates : useful cross-check

ideal  
monodisperse

## Porod invariant and volume

Following the Parseval theorem for Fourier transformations

$$Q = \int_0^{\infty} s^2 I(s) ds = 2\pi^2 \int_V (\Delta\rho(\mathbf{r}))^2 d\mathbf{r}$$

**Q** is called the Porod invariant, which is computed from the intensity but provides the mean square electron density contrast.

For homogeneous particles,  $Q=2\pi^2(\Delta\rho)^2V$ , and, taking into account that  $I(0)=(\Delta\rho)^2V^2$ , the excluded volume of hydrated particle in solution (Porod volume) is

$$V=2\pi^2 I(0)/Q .$$

## The asymptotic regime : Porod law

Integrating the Fourier transformation for  $I(s)$  by parts and using that for particles with a *sharp interface*  $\gamma'(D_{max}) = 0$ , one has

$$I(s) \cong 8\pi s^{-4} \gamma'(0) + O_1 s^{-3} + O_2 s^{-4} + o(s^{-5})$$

where  $O_1, O_2$  are oscillating trigonometric terms of the form  $\sin(sD_{max})$ . The main term responsible for the intensity decay at high angles is therefore proportional to  $s^{-4}$ , and this is known as Porod's law (1949). For homogeneous particles,  $\gamma'(0)$  is equal to  $-(\Delta\rho)^2 S/4$ , where  $S$  is the particle surface.

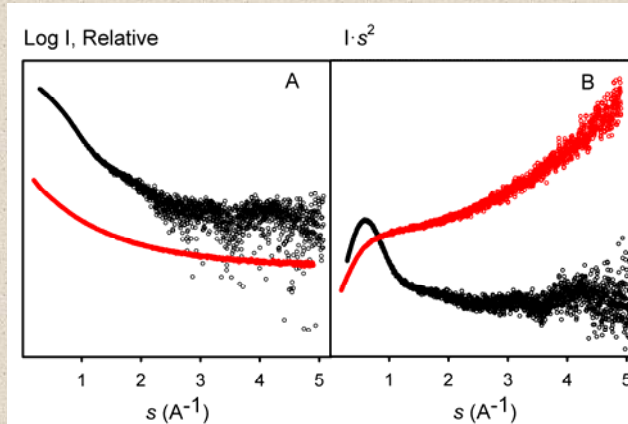
ideal  
monodisperse

## Kratky plot

A plot of  $s^2 I(s)$  vs  $s$  provides a sensitive means of *monitoring the degree of compactness* of a protein.

Globular particle :  
bell-shaped curve

Unfolded particle:  
plateau or increase  
at large  $s$ -values



## Summary of model-independent information

$I(0)/c$ , i.e. molecular mass (from Guinier plot or  $p(r)$  function)

Radius of gyration  $R_g$  (from Guinier plot or  $p(r)$  function)

Radii of gyration of thickness or cross-section (anisometric particles)

Second virial coefficient  $A_2$  (extrapolation to infinite dilution)

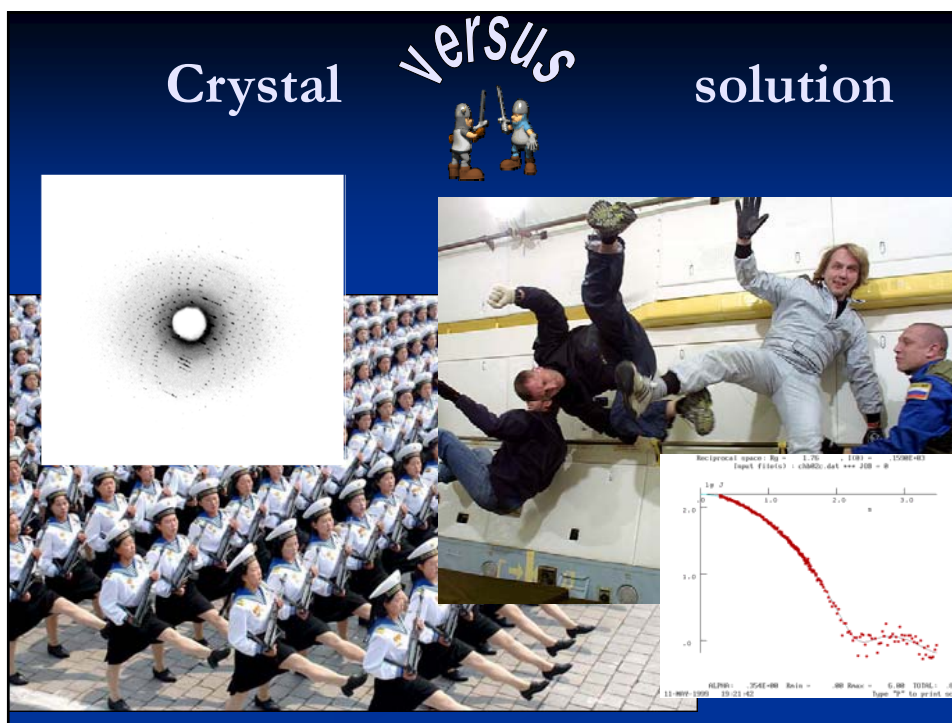
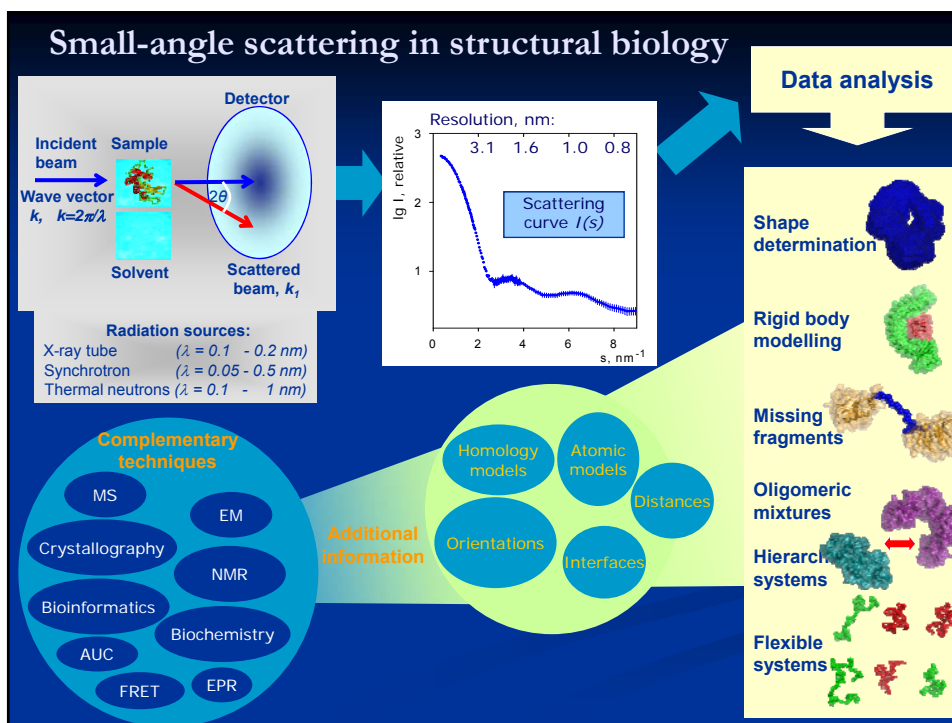
Maximum particle size  $D_{\max}$  (from  $p(r)$  function)

Particle volume  $V$  (from  $I(0)$  and Porod invariant)

Specific surface  $S/V$  (from  $I(0)$ , Porod invariant and asymptotics)

Globular or unfolded (From Kratky plot)





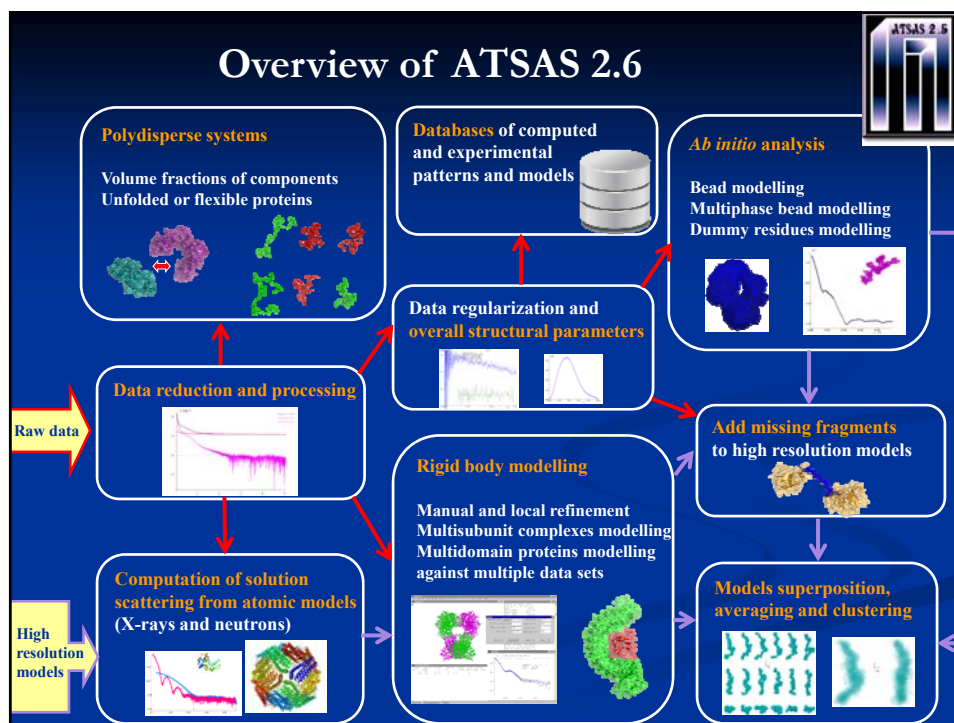
# Crystal *versus* solution





- In solution, no crystallographic packing forces are present

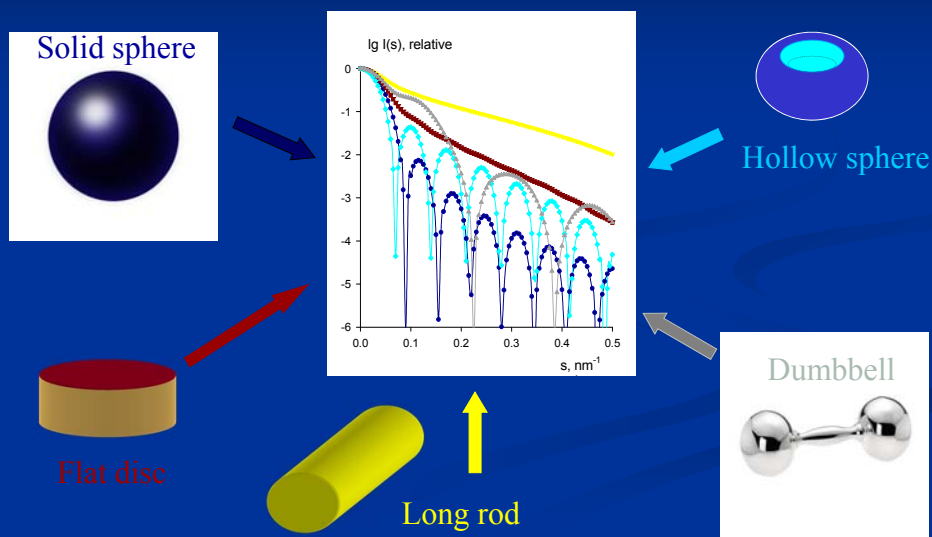
- For SAXS solution studies, one does not need to grow crystals
- SAXS is not limited by molecular mass and is applicable under nearly physiological conditions
- Using solution SAXS, one can more easily observe responses to changes in conditions
- SAXS permits for quantitative analysis of complex systems and processes



## *Data processing*

**PRIMUS:** data manipulations  
**GNOM:** distribution functions  
**BODIES:** simple shapes

The scattering is related to the shape  
(or low resolution structure)



## Recent reviews on solution SAS

Blanchet CE, Svergun DI (2013) Small-angle X-ray scattering on biological macromolecules and nanocomposites in solution. *Annual Review of Physical Chemistry* 64(1): 37–54.

Schneidman-Duhovny D, Kim S, Sali A. (2012) Integrative structural modeling with small angle X-ray scattering profiles. *BMC Structural Biology* 12(1):17.

Graewert MA, Svergun DI (2013) Impact and progress in small and wide angle X-ray scattering (SAXS and WAXS). *Curr Opin Struct Biol* 23: 748-754.

Rambo RP and Tainer JA (2013) Super-resolution in solution X-ray scattering and its applications to structural systems biology., *Annu Rev Biophys.* 42, 415-441

## Books on SAXS

"The origins" (no recent edition) : *Small Angle Scattering of X-rays*. A. Guinier and A. Fournet, (1955), in English, ed. Wiley, NY

*Small-Angle X-ray Scattering*: O. Glatter and O. Kratky (1982), Academic Press. PDF available on the Internet at <http://physchem.kfunigraz.ac.at/sm/Software.htm>

*Structure Analysis by Small Angle X-ray and Neutron Scattering*. L.A. Feigin and D.I. Svergun (1987), Plenum Press. PDF available on the Internet at [http://www.embl-hamburg.de/ExternalInfo/Research/Sax/reprints/feigin\\_svergun\\_1987.pdf](http://www.embl-hamburg.de/ExternalInfo/Research/Sax/reprints/feigin_svergun_1987.pdf)

*Small Angle X-Ray and Neutron Scattering from Solutions of Biological Macromolecules*. D.I. Svergun, M.H.J. Koch, P.A. Timmins, R.P. May (2013) Oxford University Press, London.